Advancement of dengue virus NS1 protein detection by 3D-nanoassembly complex gold nanoparticles utilizing competitive sandwich aptamer on disposable electrode

SURE 静岡大学学術リポジトリ Shizuoka University REpository

メタデータ	言語: eng
	出版者:
	公開日: 2022-04-25
	キーワード (Ja):
	キーワード (En):
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URL	http://hdl.handle.net/10297/00028941

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#### ABSTRACT 27

Signal amplification have been centralized in developing the biosensor for analyte 28 29 detection with high reliability and narrow detection window. We proposed an aptasensor to provide a highly sensitive early-stage diagnostic platform of dengue virus NS1 protein 30 (DENV-NS1) by dual-approach – colorimetric and electrochemical detection. This work 31 utilized two different aptamers specific to DENV-NS1: One conjugated to gold 32 nanoparticles (AuNPs), forming AuNPs-Apt1 and its complementary sequence aptamer, 33 forming AuNPs-Apt<sub>2</sub>. The unbound Apt<sub>1</sub> of AuNPs-Apt<sub>1</sub> by DENV-NS1 were to 34 hybridize to AuNPs-Apt2 and induced a 3D-nanoassembled formation, resulting in 35 DENV-NS1 concentration-dependent plasmonic color change. Occurrence of the 36 hybridization of Apt1 and Apt2, the 3D-assembled hybridized aptamers of AuNPs was 37 38 incubated with methylene blue (MB) solution, which intercalated a high number of MB molecules within the duplex structure of aptamers, and the complex was captured on the 39 40 Apt<sub>2</sub>-conjugated disposable gold electrode (DGE). The developed aptamer-based biosensor showed high sensitivity with colorimetric response down to 1.28 pg/mL and 41 42 electrochemical approach down to 30 fg/mL of DENV-NS1 with good selectivity. This work showcases an advanced utilization of aptamer and its complementary anti-sense 43 aptamer in signal amplification and nanocarrier for biosensing. 44

Keywords: gold nanoassembly, aptamer biosensor, colorimetric electrochemical, dengue 45 virus NS1, redox nanocarrier 46

#### 47 **1. Introduction**

In the last decades, dengue virus (DENV) infection has been a significant global 48 health issue in tropical and sub-tropical countries worldwide [1]. This mosquito-borne 49 50 viral infection disease is predicted to expand and continue to threaten more lives due to global warming, urbanization, and climate change [2]. Henceforward, tropical infectious 51 diseases should have been an anticipated threat globally [3]. Currently, the available 52 53 methods used for detecting DENV rely on cell culture [4], PCR [5] and ELISA assays [6]. 54 These conventional diagnosis methods require sophisticated medical facilities as well as 55 trained personnel which are not likely suitable for resource-limited settings [7]. Moreover, DENV is low in particle number during its earlier infection stage, which is a bottleneck 56 for early detection [8, 9]. As an alternative, the non-structural protein 1 (NS1) protein of 57 DENV (DENV-NS1) can be used because it holds clinical significance in the early phase 58 [10, 11, 12]. 59

Emerging aptamers-based biosensors (aptasensors) have attracted intensive 60 attention in disease diagnostics, environmental monitoring, and surveillance of viral 61 agents [13, 14, 15]. Presently, aptamers, a single-stranded oligonucleotide, have been 62 progressively utilized in various fields due to their specific binding with their 63 64 corresponding target with high affinity. Besides, aptamer possesses several advantages such as ease of chemical functionalization, high stability, and low cost with a little batch-65 to-batch variation [16]. In terms of simplicity, colorimetric-based aptasensors have been 66 a preferable analytical methods that have been developed using nanozyme [17], localized 67 surface plasmon resonance shift of plasmonic nanomaterial [18], and magnetic 68 nanoparticles [18]. On the contrary, electrochemical-based aptasensor has recently 69 dominated due to its higher signal-transducing properties [19, 20]. Unfortunately, the 70

developed methods only provided a single modality assay and may suffer from a lack of
signal amplification to establish a highly sensitive detection [21, 22].

Several pioneering works utilized liposomal nanoencapsulation to bring 73 multimodal sensing probes into the detection platform, combining optical and 74 electrochemical signal molecules [23, 24]. However, the existing nanocarrier has a 75 drawback of its encapsulation uniformity and prolonged protocol due to intermediate 76 77 steps to activate the sensing probes inside the nanostructure. Conversely, in the previously reported works, utilizing the nanocarrier concept has opened a new approach in 78 79 developing biosensors to overcome the urgent demand on a wide dynamic range of detection with more complementary information [15, 25]. Observing the need for more 80 straightforward detection with higher signal enhancement from the preceding works, a 81 82 feasible embodiment of intrinsic nanomaterial properties and utilization of nanocarrier are demanded to escalate the performance of the aptasensor. 83

84 Gold nanoparticles (AuNPs) have been known to undergo a versatile and easy conjugation of aptamer [26]. Herein, a dual-approach aptasensor was developed to 85 86 convey a more comprehensive dynamic range of individual detection platforms with a combined feature, highly sensitive detection from an electrochemical signal, and a simple 87 88 readout from an improved visual change. Coupling of both concepts, nanocarrier and sense-antisense competitive hybridization, the aptasensor was designed and developed to 89 90 exhibit a competitive colorimetric detection of DENV-NS1 aiming at early-diagnostic, 91 highly sensitive detection of DENV infection. Unlike a conventional single AuNPs-Apt [27], the competitive complementary AuNPs-Apt induced a 3D-nanoassembly structure 92 of AuNPs which demonstrated a higher plasmonic color shift. Different from the general 93

94 electrochemical aptasensor using an individual conjugated redox probe [28], this finding exploited a nanocarrier-based electrochemical detection by incorporating methylene blue 95 96 (MB) in the 3D-nanoassembly structure via MB-duplex aptamer interaction. The electrochemical signal from MB proved that it could enhance the detection signal down 97 98 from picogram to femtogram level. Excitingly, the developed dual-approach aptasensor provided an advanced tool for a sensitive, simple, and label-free DENV-NS1 detection 99 100 which holds great potential in an early-diagnostic biosensor to target infectious viruses 101 that are very low concentration in the early infection stage.

102

#### **103 2. Materials and methods**

104

2.1. Materials, Instruments, and Preparation of Aptamer conjugated AuNPs (Apt<sub>1</sub>- and
Apt<sub>2</sub>-conjugated AuNPs)

All the above methods are described in detail in SI-1 Material and Instruments of
the Supplementary data.

109

110 2.2. Detection of dengue virus 2 NS1 protein in buffer and spike solution

111 2.2.1. Colorimetric detection

112 Dengue virus type 2 NS1 protein (DENV-NS1) was diluted to a series of 113 concentrations. A 50  $\mu$ L of the DENV-NS1 was mixed into PBS buffer containing MgCl<sub>2</sub> 114 (1:1 v/v), and 100  $\mu$ L of AuNPs-Apt<sub>1</sub> was added into the DENV-NS1 solution. The mixture was incubated for the binding of Apt<sub>1</sub> to the DENV-NS1. The visual color and
absorbance were recorded. Next, the mixture was added with 50 µL AuNPs-Apt<sub>2</sub> solution.
The mixture was incubated to bind Apt<sub>1</sub> of the AuNPs-Apt<sub>1</sub> and Apt<sub>2</sub> of AuNPs-Apt<sub>2</sub>. For
the analysis, A<sub>525</sub> and A<sub>624</sub> were recorded as the ratio parameter of the detection plot.

#### 119 *2.2.2. Electrochemical detection*

120 The electrochemical detection was conducted on an Apt<sub>2</sub>-modified disposable gold 121 electrode (DGE). Apt<sub>2</sub>-modified DGE was prepared by incubating 10 µL of 1 µM thiol-122 functionalized Apt<sub>2</sub>. To translate the aptasensor into an electrochemical detection, the 123 AuNPs-Apt complex solution was added with 10 mM methylene blue (MB) solution (1:1 v/v). After incubation, the 15 µL mixture was drop-casted on the Apt<sub>2</sub>-modified DGE. 124 Afterward, the solution was discarded, and the DGE was washed several times with PBS 125 buffer containing 1 mM MgCl<sub>2</sub>. The working solution for the electrochemical detection 126 127 is PBS buffer with an additional 0.5 M NaCl. The differential pulse voltammetry (DPV) analysis was conducted from -0.5 V to +0.2 V at a step potential of 25 mV/s and 128 modulation pulse and time of 50 mV and 50 ms, respectively. The obtained oxidation 129 peak of the DPV was used as the electrochemical signal. 130

131

#### 132 **3. Results and discussion**

133

## 134 *3.1. Mechanism of the 3D-nanoassembled gold nanoparticles aptasensor*

The proposed aptasensor was designed based on the aptamer-conjugated AuNPs,
forming a competitive binding of AuNPs-Apt<sub>1</sub> to DENV-NS1 and its complementary

towards AuNPs-Apt<sub>2</sub>. The detection mechanism was designed in two approaches; 137 colorimetric detection and electrochemical detection, as illustrated in Scheme 1. First, 138 139 AuNPs-Apt1 were added into the detection sample and bound to the DENV-NS1 via aptamer-DENV-NS1 affinity (A). In the presence of DENV-NS1, AuNPs-Apt1 will bind 140 141 to the target DENV-NS1, forming AuNPs-Apt<sub>1</sub>/DENV-NS1 (B). Next, the proposed 142 aptasensor was added the complementary AuNPs-Apt<sub>2</sub> (C) to bind to the unbound Apt<sub>1</sub> of AuNPs-Apt1, forming AuNPs-Apt1/AuNPs-Apt2 3D-nanoassembled aggregation 143 144 (AuNPs-Apt complex) via Apt<sub>1</sub>-Apt<sub>2</sub> hybridization (**D**). The induced aggregation 145 demonstrated the color change depending on the degree of aggregation, which would also 146 be dependent on the DENV-NS1 binding to the Apt1 on the AuNPs-Apt1 (AuNPs-Apt 147 complex-based detection).

148

#### <Scheme 1>

To utilize the 3D-nanoassembled AuNPs-Apt for electrochemical detection, the 149 methylene blue (MB) was added into the AuNPs-Apt complex and bound to the duplex 150 structure of the AuNPs-Apt complex by electrostatical intercalation [29]. Then, on the 151 152 surface of the DGE, the immobilized Apt<sub>2</sub> aptamer conjugated with the unbound Apt<sub>1</sub> of 153 AuNPs-Apt complex, forming the captured DGE/Apt<sub>2</sub>/AuNPs-Apt<sub>1</sub>(AuNPs-Apt<sub>2</sub>)(DENV-NS1). The MB amount is corresponding to the amount of the hybridized 154 complex of Apt<sub>1</sub> and Apt<sub>2</sub> within the 3D-nanoassembly, inversely proportional to the 155 156 DENV-NS1 concentration in the sample solution. As the free MB was washed out, the oxidation peak in the DPV analysis indicates the amount of MB carried by the AuNPs-157 158 Apt complex only.

160 3.2. Characterization of the AuNPs-Apt<sub>1</sub>, AuNPs-Apt<sub>2</sub>, and 3D-nanoassembled AuNPs161 Apt complex

Aptamers were conjugated to AuNPs by affinity binding as illustrated in Fig. 1A. 162 AuNPs-Apt1 was prepared by conjugating biotin-functionalized Apt1 with streptavidin-163 functionalized AuNPs and AuNPs-Apt<sub>2</sub> was prepared by indirect method, conjugating via 164 Au-thiol coordination between AuNP with thiolated Apt<sub>2</sub>. To confirm the conjugation of 165 166 the AuNPs-Apt, both functionalized AuNPs were characterized by absorbance, as shown in Fig. 1B. After conjugation with Apt<sub>1</sub> and Apt<sub>2</sub>, AuNPs retain their plasmonic properties 167 168 with peaks at 525 nm with no visible shoulder. In contrast to the single AuNPs-Apt, the mixture demonstrated a change of the absorbance spectra with lower absorbance at 525 169 nm and immersed the secondary broad peak near 616 nm, indicating the aggregation 170 171 formation of AuNPs [30]. The image (inset of Fig. 1B) shows that AuNPs-Apt1 and AuNPs-Apt<sub>2</sub> have red-pinkish color, but the AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> have a blue color, 172 173 fading in a longer incubation time.

174

#### <Figure 1>

The mixture of AuNPs-Apt1 and AuNPs-Apt2 was analyzed under transmission 175 176 electron microscopy (TEM) to understand the morphology of the aggregation of the AuNP. As shown in Fig 1C, at first, AuNPs-Apt<sub>1</sub> was visibly well-dispersed with the size 177 of 20 nm. After 5 min, the interaction of AuNPs-Apt1 and AuNPs-Apt2 was demonstrated 178 by the initiation of the agglomeration of AuNPs. The aggregation of the AuNPs was 179 evitable in the presence of two AuNPs-Apt. In the conjugation of AuNP-Apt, the size of 180 two AuNPs were different; 20 nm for Apt whereas 5 nm for Apt<sub>2</sub>. Due to the difference 181 of AuNPs' sizes, the time course TEM analysis was clearly visible in TEM images (Fig. 182

183 **1D**). In the initial time, single AuNPs-Apt<sub>1</sub> with a size of 20 nm was bound to the individual of AuNPs-Apt<sub>2</sub> with a distinct size of 5 nm. In the longer incubation period, 184 185 the agglomeration of the combination of 20 nm and 5 nm of AuNPs was clearly visible. Finally, a particular agglomeration degree was observed at a prolonged time where the 186 AuNPs-Apt<sub>1</sub> was shown to be surrounded and bounded by the AuNPs-Apt<sub>2</sub>, bridging the 187 188 AuNPs via aptamer and its anti-sense aptamer [31, 32]. It is expected that the AuNPs-Apt<sub>1</sub> and AuNPs-Apt<sub>2</sub> should be capable to bind each other in three-directional formation, 189 190 resulting the 3D-nanoassemble network of AuNPs.

191

192 3.3. The colorimetric detection of DENV-NS1 using the plasmonic shift of AuNPs193 Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> aptasensor

The incubation time of AuNPs-Apt<sub>1</sub> were optimized to obtain the highest signal 194 195 of colorimetric change (Fig. S1). As the incubation time was increased, the binding of 196 AuNPs-Apt<sub>1</sub> was elevated and reached the saturation at 20 min for binding DENV-NS1 (Fig. S1A) and the average of 5 min for the AuNPs-Apt<sub>2</sub> (Fig. S1B). The colorimetric 197 198 detection of the DENV-NS1 was conducted by a series of concentration of the target analyte. The detection was done starting from the binding step of AuNPs-Apt1 to DENV-199 200 NS1 and continued to binding of AuNPs-Apt<sub>2</sub> to the free Apt<sub>1</sub> on AuNPs-Apt<sub>1</sub>. As shown in Fig. 2A, AuNPs-Apt<sub>1</sub> shows a single peak at 525 nm. With the increasing concentration 201 202 of DENV-NS1, the intensity of the shoulder peak at around 624 nm was also increasing. 203 In addition, the slight shift of the peak maxima was also observed increasing with the 204 DENV-NS1 concentration. Extending from the interaction of AuNPs-Apt<sub>1</sub>-DENV-NS1, AuNPs-Apt<sub>2</sub> was introduced to the mixture and intensified the change of the absorbance 205

206 spectrum. AuNPs-Apt<sub>2</sub> with no DENV-NS1 in the mixture (blank) has elevated shoulder 207 spectra with the lowest absorbance peak at 525 nm (Fig. 2B). These were different in 208 reverse to the AuNPs-Apt1 after the DENV-NS1 addition. In the addition of AuNPs-Apt2, the agglomeration of the AuNPs-Apts was promoted since both aptamers would undergo 209 210 hybridization and lead the 3D-nanoassembly structure of AuNPs [33]. Opposite to the previous trend the interaction of AuNPs-Apt1 and DENV-NS1, the absorbance showed 211 212 lower shoulder absorbance with the increasing concentration of DENV-NS1. The 213 absorbance at 525 nm was higher than the control, indicating less aggregation of AuNPs in the system, indicating that the conjugation between AuNPs-Apt<sub>1</sub> and DENV-NS1 was 214 215 less after-binding to the AuNPs-Apt<sub>2</sub>. TEM analysis of the AuNPs-Apt<sub>1</sub>/DENV-NS1 and 216 AuNPs-Apt<sub>2</sub> was shown in Fig. S2. Compared to the 3D-nanoassembly formation, the presence of DENV-NS1 prior to the addition of AuNPs-Apt<sub>2</sub> leads to the smaller 3D-217 nanoassembly formation, preventing to make aggregation of AuNP. 218

219

#### <Figure 2>

220 The ratio of  $A_{525}/A_{624}$  was plotted from the absorbance spectra as the function of 221 DENV-NS1 concentration. As shown in Fig. 2C, it showed an opposite correlation of the absorbance change of AuNPs-Apt1 between with the presence of the DENV-NS1, 222 223 showing positive function, and with the presence of both DENV-NS1 and AuNPs-Apt<sub>2</sub>, showing negative function. Based on the absorbance ratio, the direct detection of DENV-224 225 NS1 using only AuNPs-Apt1 showed a detection limit (LOD) of 124.83 pg/mL, based on 226 the 3 times standard deviation and blank signal according to the linearity of the aptasensor [34]. However, the competitive detection by AuNPs-Apt<sub>2</sub> could demonstrate lower LOD, 227 down to 1.28 pg/mL DENV-NS1. Moreover, comparatively to the conventional single 228

aptamer-based aptasensor, AuNPs-Apt complex competitive formation resulted to 229 distinguishable color visual in the presence of the DENV-NS1 by naked eye observation 230 231 (Fig. 2D). Moreover, after 3.5 weeks of storage, the color change of the AuNPs-Apt<sub>1</sub> did not show any observable change, but AuNPs-Apt<sub>2</sub> did undergo a minor decrease down to 232 233 a 2.5% change of absorbance (Fig. S3A). The complex AuNPs-Apt was still considerably functional, with detection only down to 6.98% (Fig. S3A). The proposed aptasensor using 234 235 additional AuNPs-Apt<sub>2</sub> as the anti-sense to promote 3D-nanoassembly of the AuNPs, the 236 advancement strategy showcases an amplified ratiometric for detecting DENV-NS1.

237

238 3.4. Electrochemical characterization of 3D-nanoassembled AuNPs-Apt as MB
239 nanocarrier

In search of a more sensitive method, DGE was used as the biosensor platform 240 241 for easy and straightforward application. First, prior to the detection, the 3D-242 nanoassembly AuNPs on the DGE was investigated whether it bound to the surface of 243 electrode. The electrochemical impedance spectroscopy (EIS) was conducted to 244 characterize the construction of the 3D-nanoassebled structure on the DGE. DGE showed 245 a typical Nyquist plot of Au-printed electrode (Fig. 3A). After the immobilization of Apt<sub>2</sub> on the DGE (DGE/Apt<sub>2</sub>), the impedance of the electrode increased. Next, AuNPs-Apt<sub>1</sub> 246 was captured on the DGE/Apt<sub>2</sub>. The layer of AuNPs covers the surface of the DGE and 247 increases its electronic properties, indicated by lower impedance. In contrast, the 248 assembled of AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> complex on the electrode resulted in higher 249 250 impedance.

The build-up network of the 3D-nanoassembly structure of AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> demonstrated different electronic properties than AuNPs-Apt<sub>1</sub>. These indicate that a single layer of AuNPs by AuNPs-Apt<sub>1</sub> had different electronic properties than a 3Dnanoassembled structure of AuNPs on the DGE by the aptamer hybridization. In addition, the presence of DENV-NS1 within the 3D-nanoassembled structure had a slightly higher impedance due to the presence of larger biomolecules, such as DENV-NS1.

Further, cyclic voltammetry was applied on the DGE to understand the redox 257 behavior on the surface of the working electrode [35]. As shown in Fig. 3B, an observed 258 peak was in the run with a potential value of around 490 mV which showed a typical 259 reduction-oxidation profile of gold printed electrode [36]. The surface of the DGE was 260 profiled to understand the difference in the presence of AuNPs-Apt1 and AuNPs-Apt2. It 261 262 was observed that DGE/Apt<sub>2</sub>/AuNPs-Apt<sub>1</sub> represented the single layer of AuNPs on the 263 DGE has a similar oxidation current like DGE/Apt. However, DGE/Apt2/AuNPs-264 Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> resulted the 3D-nanoassembly AuNPs to isolate DGE's surface and 265 unexpectedly lowered the electrons current on the surface of the electrode and reduced the oxidation peak in the cyclic voltammetry profile. 266

267

#### <Figure 3>

In this mechanism, AuNPs-Apt was acted as nanocarrier for the redox probe, MB in the electrochemical detection. To investigate this, prior to the incubation of AuNPs-Apt<sub>1</sub> and AuNPs-Apt<sub>2</sub> on the DGE/Apt<sub>2</sub>, the AuNPs-Apt was incubated in MB solution where the maximum amount of MB can be intercalated inside the aptamer. The loaded amount of the MB was determined from the current value generated in DPV analysis [37] (**Fig. 3C**). The standard oxidation peak of the MB was founded at -0.28 mV [38]. As 274 Apt<sub>2</sub> was bound to DGE directly, MB molecules chelated and showed higher DPV current than unmodified DGE, increasing from  $-3 \mu A$  to  $-4.5 \mu A$  in intensity. This indicates 275 276 that the Apt<sub>2</sub> was conjugated successfully, and MB was chelated on the capture probe. This is determined here as the noise/background signal in the electrochemical detection. 277 Further, in the presence of captured AuNPs-Apt on the surface of DGE/Apt<sub>2</sub>, the DPV 278 analysis indicated a high signal of MB in DGE/Apt<sub>2</sub>/AuNPs-Apt<sub>1</sub> and DGE/Apt<sub>2</sub>/AuNPs-279 Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> with the current intensity of  $-16 \mu$ A and  $-27 \mu$ A, respectively. Based 280 281 on the preliminary study from the MB within the AuNPs-Apt, the signal-to-noise ratio was calculated around 3-fold for AuNPs-Apt1-based nano-assembly and 6-fold for 282 AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub>-based 3D-nanoassembly structure. These signals were 283 284 demonstrated to be 2.4% in coefficient of variance on 10 independent DGEs, showing an appropriate signal transducer for the electrochemical aptasensor (Fig. S4). In a control 285 286 experiment of AuNPs-Apt nanoassembly in absence of MB, it was observed an ignorable 287 hump of oxidation current between potential value of -250 mV to -450 mV (Fig. 3D), like the bare DGE's potential value with the current around  $-2.5 \,\mu$ A. It is clearly shown 288 that the MB as a redox probe is the only responsible source of current in this 289 290 electrochemical detection.

291

3.5. The electrochemical detection of DENV-NS1 using the AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub>
aptasensor

The electrochemical detection of the DENV-NS1 was carried out after incubating the AuNPs-Apt complex/DENV-NS1 in MB solution. MB's oxidation peak was observed at potential around – 250 mV shown in **Fig. 4A**. As the concentration of the DENV-NS1 297 increased, the differential current, known as I delta in DPV analysis ( $\Delta I$ ), increased. Moreover, it was observed the dominant peak from - 250 mV was coupled to peak at 298 299 potential around -320 mV which represents the MB contribution on DGE. A higher concentration of the DENV-NS1 was resulted to lower the oxidation peak in the DPV, 300 while increasing the I delta value from negative value to less negative value. In absence 301 302 of target, the conjugated aptamers-AuNPs contain maximum number of MB, resulting 303 strong peak at -250 mV. After gradual increase of DENV-NS1, the peak of MB was 304 decreasing gradually and shifted towards -320 mV, which is the signal of DGE, in presence of MB. In case of high concentration of target DENV-NS1, all apt<sub>1</sub> are 305 306 completely blocked and there is no space for MB loading on the electrode surface. As a 307 result, the peak intensity in DPV is almost insignificant like the bare electrode without MB. The change of I delta ( $\Delta I - \Delta I_{blank}$ ) at -250 mV was plotted as the function of the 308 concentration of DENV-NS1 (Fig. 4B). The proposed aptasensor demonstrated a linear 309 detection of 1 pg/mL - 1 ng/mL DENV-NS1 with  $R^2 = 0.992$ . However, over 1 ng/mL 310 DENV-NS1 concentration, it showed to be saturated with a higher cluttering signal 311 observed in a higher-level concentration, where the detection limit was calculated 30 312 313 fg/mL, which is 100-times lower than the colorimetric detection. This result emphasizes 314 the advantage of the 3D-nanoassembly structure of AuNPs-Apt as a nanocarrier in the 315 electrochemical detection. A comparative study on previously published works were summarized in Table S1 [39-41], showing that the detection limit of the proposed 316 aptasensor was superior in terms of detection limit and dynamic range. 317

318

<Figure 4>

319 The selectivity of this dual detection was assayed in 100 pg/mL different non-320 target analytes, including norovirus-like particles (NoV-LPs), inactivated Influenza virus 321 A/H1N1 and A/H3N2. As shown in Fig. 4C, there is a slight change of signal ranging from 98% – 102% based on the blank solution in either of the non-target analytes. 322 323 However, in the presence of target analytes of 100 pg/mL DENV-NS1, the signal was changed to 80% for colorimetric detection and 40% for electrochemical detection. It 324 showed that even in a picogram concentration of target, electrochemical detection could 325 326 demonstrate a good specificity towards DENV-NS1. Further, in the spike solution of 2% 327 human serum, the proposed aptasensor could perform well for DENV-NS1 detection with 328 a relative standard deviation (RSD) ranging from 6.1% to 10.2% (Table S2), which was 329 acceptable as the detection variance. However, despite a considerably low RSD value, the developed aptasensor still showed an interfering effect in serum, probably coming 330 331 from the buffer constituents and the lysate-derived proteins [42]. It was recommendable 332 to minimize the interferences by employing up to 50-fold dilution in the biological complex matrix virus detection as for a pre-treatment and pre-dilution in the practical use. 333

334

#### 335 4. Conclusions

This work reported a dual-detection aptasensor utilizing aptamers-conjugated AuNPs to amplify the signal by 3D-nanoassembled formation. By introducing hybridized duplex aptamer as a bridge of plasmonic aggregation, the 3D-nanoassembled formation intensified the visual color change and provided a nanocarrier function for electrochemical detection. The DENV-NS1 was detected by the disruption of the duplex formation which would prevent the plasmonic color change and redox nanocarrier's moiety of the 3D-nanoassembled AuNPs. It showcased a LOD down to 1.28 pg/mL in
colorimetric and 30 fg/mL in electrochemical approaches. Considering the mechanism of
the signal amplification, the developed strategy aimed to deliver an elevated concept of
the general approach in aptamer-based detection and establishing an early-diagnostic
method in low virus concentration or low available biomarker.

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## 8 CRediT authorship contribution statement

349 Indra Memdi Khoris: Conceptualization, Methodology, Writing – original draft.
350 Fahmida Nasrin: Methodology, Writing – review & editing. Ankan Dutta
351 Chowdhury: Data interpretation, data analysis, Writing – review & editing. Enoch Y.
352 Park: Conceptualization, Writing – review & editing, Supervision.

353

#### **354 Declaration of competing interest**

The authors declare that they have no competing financial interest or personal relationships that could have appeared to influence the work reported in this paper.

357

#### 358 Acknowledgment

IMK sincerely thank the Japan Society for the Promotion of Science (JSPS) for
a research fellowship-DC (20J22358). This work was partially supported by the Fund

- 361 for the Promotion of Joint International Research, Fostering Joint International Research
- B (Grant No. 20KK0115) and the Japan Agency for Medical Research and

363 Development (20hm0102080h0001).

#### 365 Appendix A. Supplementary data

- 366 Comparison of dengue virus NS1 detection with previously published works,
- 367 detection of dengue virus NS1 spike samples in human serum, optimization of the
- aptasensor, and TEM of dengue virus NS1 conjugated to AuNPs-Apt nanoassembly.
- 369 Supplementary data to this article can be found, in the online version, at doi:https://doi:
- 370

#### 371 **References**

- [1] N. Yanagisawa, K. Wada, J.D. Spengler, R. Sanchez-Pina, Health preparedness plan
   for dengue detection during the 2020 summer Olympic and Paralympic games in
   Tokyo, PLoS Negl.Trop. Dis., 12 (2018) e0006755.
- [2] F.J. Colón-González, M.O. Sewe, A.M. Tompkins, H. Sjödin, A. Casallas, J. Rocklöv,
  et al., Projecting the risk of mosquito-borne diseases in a warmer and more
  populated world: a multi-model, multi-scenario intercomparison modelling study,
  The Lancet Planetary Health, 5 (2021) e404–e414.
- [3] M.A. Kabir, H. Zilouchian, M.A. Younas, W. Asghar, Dengue Detection: Advances
  in Diagnostic Tools from Conventional Technology to Point of Care, Biosensors,
  11 (2021) 206.
- [4] E. Iswardy, T.-C. Tsai, I.-F. Cheng, T.-C. Ho, G.C. Perng, H.-C. Chang, A bead-based
  immunofluorescence-assay on a microfluidic dielectrophoresis platform for rapid
  dengue virus detection, Biosens. Bioelectron., 95 (2017) 174–180.
- [5] P.R. Abraham, R. Bharathy, P. Kumar, A. Kumar, Dengue NS1 antigen kit shows
  high sensitivity for detection of recombinant dengue virus-2 NS1 antigen spiked
  with Aedes aegypti mosquitoes, Sci. Rep., 11 (2021) 23699.
- [6] A. Vázquez-Guardado, F. Mehta, B. Jimenez, A. Biswas, K. Ray, A. Baksh, et al.,
   DNA-Modified Plasmonic Sensor for the Direct Detection of Virus Biomarkers
   from the Blood, Nano Lett., 21 (2021) 7505–7511.
- [7] R. Eivazzadeh-Keihan, P. Pashazadeh-Panahi, T. Mahmoudi, K.K. Chenab, B.
  Baradaran, M. Hashemzaei, et al., Dengue virus: a review on advances in detection
  and trends-from conventional methods to novel biosensors, Microchim. Acta, 186
  (2019) 3249.
- [8] S.-C. Lai, Y.-Y. Huang, P.-Y. Shu, S.-F. Chang, P.-S. Hsieh, J.-J. Wey, et al.,
  Development of an enzyme-linked immunosorbent assay for rapid detection of
  dengue virus (DENV) NS1 and differentiation of DENV serotypes during early
  infection, J. Clin. Microbiol., 57 (2019) e00221–00219.

- [9] O. Parkash, M.A. Abdullah, C.Y. Yean, S.D. Sekaran, R.H. Shueb, Development and
   Evaluation of an Electrochemical Biosensor for Detection of Dengue-Specific IgM
   Antibody in Serum Samples, Diagnostics, 11 (2021) 33.
- 402 [10] A. Dhal, T. Kalyani, S. Ghorai, N.K. Sahu, S.K. Jana, Recent development of
  403 electrochemical immunosensor for the diagnosis of dengue virus NSI protein: A
  404 review, Sensors International, (2020) 100030.
- [11] D. Wasik, A. Mulchandani, M.V. Yates, Point-of-use nanobiosensor for detection of
   dengue virus NS1 antigen in adult Aedes aegypti: a potential tool for improved
   dengue surveillance, Anal. Chem., 90 (2018) 679–684.
- 408 [12] P.P.A. Suthanthiraraj, A.K. Sen, Localized surface plasmon resonance (LSPR)
  409 biosensor based on thermally annealed silver nanostructures with on-chip blood410 plasma separation for the detection of dengue non-structural protein NS1 antigen,
  411 Biosens. Bioelectron., 132 (2019) 38–46.
- [13] X. Liu, H. Zhang, S. Qin, Q. Wang, X. Yang, K. Wang, Optical fiber amplifier for
  quantitative and sensitive point-of-care testing of myoglobin and miRNA-141,
  Biosens. Bioelectron., 129 (2019) 87–92.
- [14] Z. Zhang, L. Dong, Q. Zhu, Rational engineering of synergically stabilized aptamer cDNA duplex probes for strand displacement based electrochemical sensors,
   Electrochim. Acta, 282 (2018) 588–594.
- [15] X. Zhang, H. Zhi, M. Zhu, F. Wang, H. Meng, L. Feng, Electrochemical/visual dualreadout aptasensor for Ochratoxin A detection integrated into a miniaturized paperbased analytical device, Biosens. Bioelectron., 180 (2021) 113146.
- [16] T.T.-Q. Nguyen, E.R. Kim, M.B. Gu, A new cognate aptamer pair-based sandwichtype electrochemical biosensor for sensitive detection of Staphylococcus aureus,
  Biosens. Bioelectron., 198 (2022) 113835.
- 424 [17] P. Weerathunge, R. Ramanathan, V.A. Torok, K. Hodgson, Y. Xu, R. Goodacre, et
  425 al., Ultrasensitive colorimetric detection of murine norovirus using NanoZyme
  426 aptasensor, Anal. Chem., 91 (2019) 3270–3276.
- [18] L. Xu, R. Chopdat, D. Li, K.T. Al-Jamal, Development of a simple, sensitive and
  selective colorimetric aptasensor for the detection of cancer-derived exosomes,
  Biosens. Bioelectron., 169 (2020) 112576.
- [19] A. Idili, C. Parolo, R. Alvarez-Diduk, A. Merkoçi, Rapid and efficient detection of
  the SARS-CoV-2 spike protein using an electrochemical aptamer-based sensor,
  ACS Sens., 6 (2021) 3093–3101.
- 433 [20] S. Sheibani, L. Capua, S. Kamaei, S.S.A. Akbari, J. Zhang, H. Guerin, et al.,
  434 Extended gate field-effect-transistor for sensing cortisol stress hormone, Commun.
  435 Mater., 2 (2021) 10.
- 436 [21] K. Takemura, A.B. Ganganboina, I.M. Khoris, A.D. Chowdhury, E.Y. Park,
  437 Plasmon Nanocomposite-Enhanced Optical and Electrochemical Signals for
  438 Sensitive Virus Detection, ACS Sens., 6 (2021) 2605–2612.
- 439 [22] A.B. Ganganboina, A.D. Chowdhury, I.M. Khoris, R.-a. Doong, T.-C. Li, T. Hara,
  440 et al., Hollow magnetic-fluorescent nanoparticles for dual-modality virus detection,
  441 Biosens. Bioelectron., 170 (2020) 112680.
- [23] A.B. Ganganboina, A.D. Chowdhury, I.M. Khoris, F. Nasrin, K. Takemura, T. Hara,
  et al., Dual modality sensor using liposome-based signal amplification technique
  for ultrasensitive norovirus detection, Biosens. Bioelectron., 157 (2020) 112169.

- [24] F. Nasrin, A.D. Chowdhury, A.B. Ganganboina, O.J. Achadu, F. Hossain, M.
  Yamazaki, et al., Fluorescent and electrochemical dual-mode detection of Chikungunya virus E1 protein using fluorophore-embedded and redox probeencapsulated liposomes, Microchim. Acta, 187 (2020) 674.
- [25] I.M. Khoris, A.B. Ganganboina, E.Y. Park, Self-Assembled Chromogenic Polymeric
   Nanoparticle-Laden Nanocarrier as a Signal Carrier for Derivative Binary
   Responsive Virus Detection, ACS Appl. Mater. Interfaces, 13 (2021) 36868–36879.
- [26] R. Gupta, A. Kumar, S. Kumar, A.K. Pinnaka, N.K. Singhal, Naked eye colorimetric
  detection of Escherichia coli using aptamer conjugated graphene oxide enclosed
  Gold nanoparticles, Sens. Actuators, B, 329 (2021) 129100.
- [27] V. Morya, S. Walia, B.B. Mandal, C. Ghoroi, D. Bhatia, Functional DNA based
  hydrogels: development, properties and biological applications, ACS Biomater. Sci.
  Eng., 6 (2020) 6021–6035.
- [28] C. Wang, Q. Zhao, A reagentless electrochemical sensor for aflatoxin B1 with
  sensitive signal-on responses using aptamer with methylene blue label at specific
  internal thymine, Biosens. Bioelectron., 167 (2020) 112478.
- 461 [29] E. Farjami, L. Clima, K.V. Gothelf, E.E. Ferapontova, DNA interactions with a
  462 methylene blue redox indicator depend on the DNA length and are sequence
  463 specific, Analyst, 135 (2010) 1443–1448.
- [30] A. Baeissa, N. Dave, B.D. Smith, J. Liu, DNA-functionalized monolithic hydrogels
  and gold nanoparticles for colorimetric DNA detection, ACS Appl. Mater.
  Interfaces, 2 (2010) 3594–3600.
- 467 [31] M.Q. He, S. Chen, K. Yao, K. Wang, Y.L. Yu, J.H. Wang, Oriented assembly of
  468 gold nanoparticles with freezing driven surface DNA manipulation and its
  469 application in SERS based MicroRNA assay, Small Methods, 3 (2019) 1900017.
- 470 [32] M. Luo, M. Xuan, S. Huo, J. Fan, G. Chakraborty, Y. Wang, et al., Four 471 Dimensional Deoxyribonucleic Acid Gold Nanoparticle Assemblies, Angew.
  472 Chem. Int. Ed., 59 (2020) 17250–17255.
- [33] M.-Q. He, S. Chen, K. Yao, J. Meng, K. Wang, Y.-L. Yu, et al., Precisely Tuning
  LSPR Property via "Peptide-Encoded" Morphological Evolution of Gold Nanorods
  for Quantitative Visualization of Enzyme Activity, Anal. Chem., 92 (2019) 1395–
  1401.
- [34] I.M. Khoris, A.B. Ganganboina, T. Suzuki, E.Y. Park, Self-assembled chromogenloaded polymeric cocoon for respiratory virus detection, Nanoscale, 13 (2021) 388–
  396.
- [35] A. Dutta Chowdhury, A.B. Ganganboina, F. Nasrin, K. Takemura, R.-a. Doong,
  D.I.S. Utomo, et al., Femtomolar detection of dengue virus DNA with serotype
  identification ability, Anal. Chem., 90 (2018) 12464–12474.
- [36] V. Rodovalho, G. Araujo, E. Vaz, C. Ueira-Vieira, L. Goulart, J. Madurro, et al.,
  Peptide-based electrochemical biosensor for juvenile idiopathic arthritis detection,
  Biosens. Bioelectron., 100 (2018) 577–582.
- [37] S. Khezrian, A. Salimi, H. Teymourian, R. Hallaj, Label-free electrochemical IgE
  aptasensor based on covalent attachment of aptamer onto multiwalled carbon
  nanotubes/ionic liquid/chitosan nanocomposite modified electrode, Biosens.
  Bioelectron., 43 (2013) 218–225.
- [38] S.M. Taghdisi, N.M. Danesh, M.A. Nameghi, M. Ramezani, M. Alibolandi, M.
   Hassanzadeh-Khayat, et al., A novel electrochemical aptasensor based on

- 492 nontarget-induced high accumulation of methylene blue on the surface of electrode
  493 for sensing of α-synuclein oligomer, Biosens. Bioelectron., 123 (2019) 14–18.
- 494 [39] A. Santos, P.R. Bueno, J.J. Davis, A dual marker label free electrochemical assay
   495 for Flavivirus dengue diagnosis, Biosens. Bioelectron., 100 (2018) 519–525.
- [40] B.B. Junior, M.R. Batistuti, A.S. Pereira, E.M. de Sousa Russo, M. Mulato,
  Electrochemical aptasensor for NS1 detection: Towards a fast dengue biosensor,
  Talanta, 233 (2021) 122527.
- [41] M.H. Nawaz, A. Hayat, G. Catanante, U. Latif, J.L. Marty, Development of a portable and disposable NS1 based electrochemical immunosensor for early diagnosis of dengue virus, Anal. Chim. Acta, 1026 (2018) 1–7.
- 502 [42] J. Tate, G. Ward, Interferences in immunoassay, The clinical biochemist reviews,
   503 25 (2004) 105.

#### 506 Figure Caption

Scheme 1. Proposed 3D-nanoassembled gold nanoparticles-based aptasensor designed

- 508 for colorimetric detection and electrochemical detection. (A) and (C) indicate AuNPs-
- 509 Apt<sub>1</sub> and AuNPs-Apt<sub>2</sub> as the detection probes; (B) shows DENV-NS1 binding to AuNPs-
- 510 Apt<sub>1</sub> and (**D**) shows 3D-nanoassembly of AuNPs; (**E**) indicates electrochemical detection
- step and (F) shows the 3D-nanoassembled AuNPs captured on the Apt<sub>2</sub>-modified DGE.
- Fig. 1. Characterization of 3D-nanoasembly aggregation of AuNPs-Apt1 and AuNPsApt2. (A) The illustration of the preparation of AuNPs-Apt1 and AuNPs-Apt2; (B)
  Absorbance and visual images of the AuNPs-Apt1 (1), AuNPs-Apt2 (2) and AuNPsApt1/AuNPs-Apt2 (3); TEM images of time-dependent nanoassembled formation of (C)
  AuNPs-Apt1 (20)/AuNPs-Apt2 (20), and (D) AuNPs-Apt1 (20)/AuNPs-Apt2 (5). The
  scale bars of the images are represented on each image.
- **Fig. 2.** The colorimetric detection of DENV-NS1 using the proposed aptasensor. The absorbance spectra of the AuNPs-Apt<sub>1</sub> after the addition of DENV-NS1 (**A**) and the addition of DENV-NS1 and AuNPs-Apt<sub>1</sub> (**B**); (**C**) indicates the comparative plot of DENV-NS1 concentration vs. ratiometric of  $A_{525}$  and  $A_{624}$  (the error bars indicate the standard errors based on three measurements); (**D**) the visual image represents the color change in determining the concentration of DENV-NS1 by the proposed aptasensor.
- Fig. 3. 3D-nanoassembly AuNPs as the nanocarrier for electrochemical performance on
  a disposable gold electrode (DGE). (A) Electrochemical Impedance Spectroscopy (EIS)
  and (B) Cyclic voltammetry (CV) of the captured AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> on Apt<sub>2</sub>-

- functionalized DGE with scan rate of 75 mV/s; Electrochemical performance of captured
  3D-nanoassembly AuNPs-Apt<sub>1</sub>/AuNPs-Apt<sub>2</sub> with MB (C) and without (D).
- **Fig. 4.** The electrochemical detection of DENV-NS1 using the proposed aptasensor on
- 530 Apt<sub>2</sub>-immobilized Disposable Gold Electrode (DGE). (A) DPV analysis of the aptasensor
- in response in the DENV-NS1 detection; (B) semi-log plot of change of differential
- 532 current ( $\Delta I$ ) vs. concentration of DENV-NS1; (C) The selectivity test of proposed
- aptasensor using colorimetric detection and electrochemical detection. The error bars in
- **B** and **C** denote the standard errors from three measurements.

#### 536 Scheme 1

#### 



#### Fig. 1

#### 







553 Fig. 4



# Supplementary data

# Advancement of dengue virus NS1 protein detection by 3Dnanoassembly complex gold nanoparticles utilizing competitive sandwich aptamer on disposable electrode

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#### **SI-1** Material and Instruments

#### SI-1.1. Materials

Two kinds of gold nanoparticles (AuNPs) (5 nm and 20 nm) were obtained from Sigma-Aldrich (St. Louis, MO, USA). Disposable gold electrode (DGE) was purchased from Metrohm Dropsens (C220-BT, Herisau, Switzerland). Streptavidin was obtained from Wako Pure Chemical (Tokyo, Japan). Anti-dengue type 2 NS1 protein aptamer (Apt1) (Sequence name: ATW0005-BY5-100) and its complementary aptamer (Apt2) were purchased from Pair Biotechnologies, Inc. (TX, USA). Apt1 and Apt2 have a length of 32 nucleotides and 14 nucleotides, respectively. Apt2 was custom ordered with 3 mismatches evenly spaced over the 14 base lengths.

Influenza virus A and its subtypes were obtained from ProSpec-Tany Technogene, Ltd. (East Brunswick, NJ, USA). Recombinant dengue virus 2 NS1 protein (ab181966) was purchased from Abcam (Cambridge, UK), and 293T whole cell lysate was obtained from Genetex (CA, USA). According to our previous work, norovirus-like particles (NoV-LPs) were prepared from a silkworm expression system [1]. All experiments were conducted using deionized (DI) and autoclaved water.

#### SI-1.2. Instruments

The absorbance was measured using a clear transparent cuvette (l = 10 mm) by UV-vis spectrophotometer (Shimadzu, Kyoto, Japan) and by using a transparent 96-wells microplate reader (INFINITE 200 M Plex, TECAN, Kanagawa, Japan). Transmission electron microscopy (TEM) images were generated using TEM (JEM-2100F, JEOL, Ltd., Tokyo, Japan) operated at 100 kV. The electrochemical measurement was conducted using Bio-Logic SP-200 Potentiostat and EC-Lab V11.02 software (Bio-Logic Sci. Instruments, Seyssinet-Pariset, France).

#### SI-1.3. Preparation of Apt<sub>1</sub>- and Apt<sub>2</sub>-conjugated AuNPs

The conjugation of the aptamers to AuNPs is based on the general streptavidin-biotin binding [2] for anti-dengue type 2 NS1 protein aptamer (Apt<sub>1</sub>) forming AuNPs-Apt<sub>1</sub>. Initially, 2 mL of AuNPs (0.5 a.u) was mixed with 50 µL streptavidin solution (1 mg/mL) and was incubated for 2 h. Then, the solution containing non-conjugated streptavidin was removed. AuNPsstreptavidin was redispersed in phosphate-buffered saline (PBS) buffer containing 1 mM MgCl<sub>2</sub>. Apt<sub>1</sub> with biotin on its 5'-end was prior resuspended and refolded according to the instructed protocol from the provider. After refolding, 5 µM of Apt<sub>1</sub> was added to the AuNPs-streptavidin and incubated for 2 h at room temperature. Afterward, the AuNPs-Apt<sub>1</sub> solution was centrifuged to remove excess aptamer. The Apt<sub>1</sub>-conjugated AuNPs (AuNPs-Apt<sub>1</sub>) were redispersed in PBS buffer containing 1 mM MgCl<sub>2</sub>.

The conjugation of AuNPs-Apt<sub>2</sub> uses a thiol-Au affinity reaction with Apt<sub>2</sub> aptamer having thiol-group at its 5'-end [3]. The conjugation was simply done by mixing AuNPs (2 mL, 0.5 a.u) and the Apt<sub>1</sub>'s complementary aptamer (Apt<sub>2</sub>) (5  $\mu$ M), and was incubated for 2 h at room temperature. Afterward, AuNPs-Apt<sub>2</sub> was redispersed in PBS buffer containing 1 mM MgCl<sub>2</sub>. According to the provider's protocol, the Apt<sub>2</sub> was priorly resuspended, refolded, and reduced.

<b>Detection Principle</b>	Conjugate	C <sub>lod</sub> (ng/mL)	Linear range (ng/mL)	Reference
Immunofluorescence	Antibody	15	15-500	[4]
Electrochemical $(EIS^{1}, SPCE^{2})$	Antibody	0.3	1–200	[5]
Electrochemical (Capacitive)	Antibody	0.34	1–5000	[6]
Electrochemical (EIS)	Aptamer	0.05	0.01-1000	[7]
Colorimetric	ELISA kit <sup>3</sup>	1	1–100	[8]
Colorimetric	ELISA kit <sup>4</sup>	$1.5 \times 10^{-2}$	_	[9]
Colorimetric	Aptamer	$1.28 \times 10^{-3}$	1 - 1000	This work
Electrochemical (DPV)	Aptamer	3.0×10 <sup>-5</sup>	0.001-1	This work

Table S1. Comparative study of the previous work related to DENV NS1 detection-

<sup>1</sup>EIS = Electrochemical Impedance Spectroscopy <sup>2</sup>SPCE = Screen-Printed Carbon Electrode

<sup>3</sup>TANAKA Kikinzoku Kogyo (TKK) ELISA kit <sup>4</sup>J. Mitra & Co. Pvt. Ltd Dengue NS1 Ag Microlisa kit in dried DENV vector (mosquito)

Table S2.	The recover	y test of the	dual-approach	of	<b>DENV-NS1</b>	in	human	serum	using
AuNPs-A	pt <sub>1</sub> /AuNPs-A	pt <sub>2</sub> based apt	asensor						

Sample No. <sup>1</sup>	DENV-NS1 concentration (pg/mL)	<b>Recovery of DENV-NS1 concentration (%)</b>						
		CL.D <sup>2</sup>	<b>RSD<sup>3</sup> (%)</b>	EC.D <sup>4</sup>	RSD (%)			
1	2500	98.6	8.50	99.4	10.20			
2	1000	112.5	6.15	120.5	8.71			
3	500	115.4	4.12	105.1	6.70			

<sup>1</sup>DENV-NS1 were spiked in 2% human serum with three independent detections for each sample.

<sup>2</sup>CL.D: colorimetric detection

<sup>3</sup>EC.D: electrochemical detection.

<sup>4</sup>RSD: relative standard deviation calculated from three samples detection.



Fig. S1. Optimization of AuNPs-Apt1 and AuNPs-Apt2 binding



Fig. S2. TEM image of AuNPs/Apt1-NS1/AuNPs-Apt2



**Fig. S3.** (A) the absorbance A<sub>532</sub> of AuNPs-Apt solution in a function of storage duration and (B) performance assessment of AuNPs-Apt during 24-day post-synthesis time.



Fig. S4. Reproducibility of the electrochemical baseline signal in 10 electrodes in DPV analysis.

#### References

- J. Boonyakida, D.I.S. Utomo, F.N. Soma, E.Y. Park, Two-step purification of tag-free norovirus-like particles from silkworm larvae (Bombyx mori), Protein Expression Purif., 190 (2022) 106010.
- [2] R. Hu, W. Wen, Q. Wang, H. Xiong, X. Zhang, H. Gu, et al., Novel electrochemical aptamer biosensor based on an enzyme–gold nanoparticle dual label for the ultrasensitive detection of epithelial tumour marker MUC1, Biosens. Bioelectron., 53 (2014) 384–389.
- [3] S. Giorgi-Coll, M.J. Marín, O. Sule, P.J. Hutchinson, K.L. Carpenter, Aptamer-modified gold nanoparticles for rapid aggregation-based detection of inflammation: an optical assay for interleukin-6, Microchim. Acta, 187 (2020) 13.
- [4] N.T. Darwish, S.D. Sekaran, Y. Alias, S.M. Khor, Immunofluorescence–based biosensor for the determination of dengue virus NS1 in clinical samples, J. Pharm. Biomed. Anal., 149 (2018) 591–602.
- [5] M.H. Nawaz, A. Hayat, G. Catanante, U. Latif, J.L. Marty, Development of a portable and disposable NS1 based electrochemical immunosensor for early diagnosis of dengue virus, Anal. Chim. Acta, 1026 (2018) 1–7.
- [6] A. Santos, P.R. Bueno, J.J. Davis, A dual marker label free electrochemical assay for Flavivirus dengue diagnosis, Biosens. Bioelectron., 100 (2018) 519–525.
- [7] B.B. Junior, M.R. Batistuti, A.S. Pereira, E.M. de Sousa Russo, M. Mulato, Electrochemical aptasensor for NS1 detection: Towards a fast dengue biosensor, Talanta, 233 (2021) 122527.
- [8] K. Suzuki, E.E. Nakayama, A. Saito, A. Egawa, T. Sato, J. Phadungsombat, et al., Evaluation of novel rapid detection kits for dengue virus NS1 antigen in Dhaka, Bangladesh, in 2017, Virol. J., 16 (2019) 102.
- [9] P.R. Abraham, R. Bharathy, P. Kumar, A. Kumar, Dengue NS1 antigen kit shows high sensitivity for detection of recombinant dengue virus-2 NS1 antigen spiked with Aedes aegypti mosquitoes, Sci. Rep., 11 (2021) 23699